1

Research Paper

2 Modeling of the effect of backpack load position on the lumbar spine curvature

3 Abstract:

4 The aim of this study was to numerically calculate the lumbar spine curvature in standing from a healthy 5 subject with a loaded backpack. The anthropometric data of a schoolboy were used, and then the 6 modelwas built in BRG.LifeMOD (ver. 2007, Biomechanics Research Group, Inc., USA) based on these 7 data. The backpack was loaded at 10, 15 and 20% of subject's Body weight (BW) (stage 1). Then, three 8 boxes (4, 4 and 12 Kg in weight) were attached in the backpack (stage 2). They were arranged in the 9 sagittal, frontal and transversal planes and the position of the heavier weight was changed at each 10 phase. Regression analysis between our numerical predictions of stage 1 and similar experimental literature led to a correlation gradient of 0.88 and 0.91 for L3-S1-horizon and T12-L3-S1 angles, 11 12 respectively. The predicted G and H angles peaks at stage 2 were observed when the heavier boxwas in 13 frontal plane at left or right side. This study demonstrated the feasibility of obtaining a range of variable 14 boundary conditions (e.g. altered due to changing the location of the heavier box) and applying a 15 simplified three-dimensional model that can predict lumbar spine curvature changes in relatively short 16 solution time.

17 Keywords: Backpack modeling, backpack Load Placement, lumbar spine curvature

18 **1. Introduction**

19 Backpack users mostlyare students, military soldiers, mountain climbers, rescueworkers,

20 recreational hikers. The average load usually moved by students is 22% of their (BW) (Motmans et

al, 2006).Naturally more than $\frac{1}{3}$ of young students can carry more than 30% of their BW.But 21 22 heavier loads for longer times are usually conveyed in industrial, military as well as recreational applications (Motmans et al, 2006). Most of the previous studies have been about 23 24 schoolbackpacks that were done empirically (Chow et al, 2007; Reid et al, 2004; Singh, T. and Koh, 2009; Stephanie et al, 2007). Currently, experimental methods are typically used to 25 determine biomechanical behaviors. However, such techniques are difficult, expensive, and 26 27 sometimes have risks connected to them (Bahraseman et al, 2013). Numerical methods, 28 although, have the potential to determine them removing the need for experimental procedures. 29 It was reported that carrying heavy backpacks might result in changes in trunk posture and 30 31 finally lower back pain (LBP)(Al-Khabbaz et al, 2008). Also prolonged carrying of backpacks 32 affects the fluid content of the intervertebral discs (Skaggs et al, 2006). The Most significant parameters were studiedbefore, include: the type of backpackand its design (Mackie et al, 33 2003; Motmans et al, 2006; Rashed et al, 2005), different weights of that [Chow et al, 2007], 34 location of its'center of gravity (COG)(Abe et al, 2008; Devroey et al, 2007; Stuempfle et al, 35 2004), lateral stiffness elements in the suspension system of a backpack (Reid et al, 2004; 36 Stephanie et al, 2007), backpack harness system [Stephanie et al, 2007; Hamish et al, 2005), 37 38 spinal muscles activities (Al-Khabbaz et al, 2008; Motmans et al, 2006), musculoskeletal symptoms (especially trunk posture) (Al-Khabbaz et al, 2008; Chow et al, 2007; Skaggs et al, 39 40 2006; Grimmer et al, 2002), gender influence (Haex, 2004), physiological parameters (Stuempfle et al, 2004), maintaining balance(Rashed et al, 2005) and comparison of static and dynamic 41 stages(Singh et al, 2009). Stuempfle et al. (2004) reported that double pack could bemore 42

physiologically efficient technique but is not easy enough. Head-loading and back-loading were 43 44 compared and the results showed that whilst back-loading weremostly associated with more areas of discomfort than head-loading(Lloyd et al, 2010). Chow et al. (2007) examined the effect 45 of increasing backpack load on the spine alignment and observed increasing trunk forward lean 46 47 (TFL) with increasing backpack load. Stuempfle et al. (2004) foundthat electromyography activity of the erector spinaeand trapezius were significantly lower when the load was located high on 48 the back.Devroey et al. (2007) reported morepostural changesat lumbar spineindynamic load 49 50 carryingthan in static condition. It was reported that the erector spinae EMG activity decreases in carrying backpack, in contrast, rectus abdominisEMG activity increases (Al-Khabbazet al, 2008; 51 52 Motmans et al, 2006). Stephanie et al. (2007) indicated that putting a hip belt in a framed backpackmay transfer about 30% of backpack vertical force to the hip. 53 The purpose of this study is to modeling of the lumbar spine curvature in standing from a 54 55 healthy subject with a loaded backpack. Firstly, the backpack is loaded at 10, 15 and 20% of subject's BW (stage 1). Secondly, three boxes (4, 4 and 12 Kg in weight) were attached in the 56 backpack (stage 2). They were arranged in the sagittal, frontal and transversal planes and the 57 position of the heavier weight was changed at each phase. 58

59

60 **2. Method**

The model was included the anthropometric data of 15.2 years old boy (1.6 m height, 58.9 kg weight).Then an adaptedschool backpack was applied to the model (Fig 1). The BRG.LifeMod software version 2005 was applied to make a model and to perform the analysis. The software

divides the spinal column intothoracic, cervical and lumbar parts and connects these three
parts by joints. Respecting to theexactnessrequired in investigating the spinal alignment, the
simulating of vertebrae has been executed to make the definition of joints between the
vertebrae possible. For all body joints, except for intervertebral disks, the standard hybrid III
values were used. To create the desired range of motion (ROM) and stiffness for vertebral
column, the natural ROM and the joint damping coefficient of the joint were input (Leilnahari et
al, 2011).

71 Design of Modeling and boundary conditions:

72 Simulation was done at two stages. At stage1, loading of backpack was modeled at 10, 15 and 20% of boy's BW by applying two single forces at the location of shoulder straps 73 symmetrically. Initially a backpack frame was built by passing a spline next to the vertebrae 74 mass centers (T_2 till L_5) on sagittal plane and a polyline adds perpendicularly on frontal plane, 75 then in MSC ADAMSversion 2005 these two frames were merged to one unit frame (Fig 1). 76 Hence, massless backpack frame were made of aluminum (density: 2740 kg/m³, young's 77 modulus: 7.1705e+010 N/m², Poisson's coefficient: 0.33). Finally, the backpack was fixed in 78 79 shoulders. The cubic volumes in MSC ADAMS 2005 were used to apply the load in the backpack. A box was attached to the backpack frame adjacent to T12 by fixed joint. At Each phase the box 80 was weighed in 10%, 15% or 20% of the boy's BW. 81 82 At stage2, The backpack included a weight within that is distributed in three boxes; they were 4, 4, and 12 kg in weight. These boxes attached to the backpack frame in three phases. At each 83 phase, boxes were arranged in parallel to the sagittal (Fig 2a), frontal (Fig 2b), and 84

transversal(Fig 2c) planes. In all phases, the location of the heavier box (12 Kg) was changed to
assess probable effects on the lumbar angle. Thus totally nine cases were examined. Table 1
provides the relevant abbreviations of The heavy box location (12 Kg) in each plane related to its
arrangement.

89

90 3. Results

91 **3.1** Investigation of G and H angles changes due to variation in load (Stage 1)

- 92 The G angle was decreased with increasing load (Table 2, Fig 3). It was ranged from 28.1 to 24.8
- 93 degree when load was changed from 0 to 20% of BW. The mean slope of G angle changes to
- 94 load variations was about -18.343 (degree/N) and the y-axis intercepts of that was 80.289
- 95 (degree). The percentage reduction of G angle was roughly 11.7.
- 96 The H angle was decreased with increasing load (Table 2, Fig 3). It was ranged from 79.1 to 75.8
- 97 degree when load was changed from 0 to 20% of BW. The mean slope of H angle changes to
- 98 load variations was about -19.486 (degree/N) and the y-axis intercepts of that was 29.417
- 99 (degree). The percentage reduction of G angle was roughly 4.2.
- 100 The relationship between G and H angle was shown in Figure 4. A good correlation was
- 101 determined using a quadratic polynomial equation, for our numerical simulations.

102 **3.2** Investigation of G and H angles changes due to variation in loadarrangement (Stage 2)

- 103 The table 3 gives information on the prediction of lumbar angles ,included G and H, when the
- 104 location of heavy box was changed at each plane. As provided in table 3, in sagittal plane, when

105	the heavy box was located at top of the other boxes (SM), the G angle was calculated 23.9
106	degree. This is the biggest calculated G angle in sagittal plane as compared to prediction of that
107	in ST(23.2 degree) and SB (22.9 degree) stages.
108	In frontal plane, when the heavy box was located at the middle of the other boxes (FM), the G
109	angle was calculated 24.4 degree (Table 3). This is the least calculated G angle in frontal plane
110	as compared to prediction of that in FLand FR stages which in bothof themthe same G angle of
111	25.1 degreewas calculated.
112	In transversal plane, when the heavy box was located at the TF stage, the G angle was
113	calculated 24.6degree (Table 3). This is the biggest calculated G angle in transversal plane as
114	compared to prediction of that in TN (24.1degree) and TM (24.4degree) stages.
115	As provided in table 3, in sagittal plane, when the heavy box was located at the middle of the
116	other boxes (SM), the H angle was calculated 74.4 degree. This is the biggest calculated H angle
117	in sagittal plane as compared to prediction of that in ST (73.4 degree) and SB (72.9 degree)
118	stages.
119	In frontal plane when the heavy box was located at the middle of the other boxes (FM), the H

In frontal plane, , when the heavy box was located at the middle of the other boxes (FM), the H angle was calculated 75.1 degree (Table 3). This is the least calculated H angle in sagittal plane as compared to prediction of that in FL and FR stages which in both of them the same G angle of 76.0 was calculated.

123	In transversal plane, when the heavy box was located at the TF stage, the H angle was
124	calculated 75.4 degree (Table 3). This is the biggest calculated H angle in transversal plane as
125	compared to prediction of that in TN (74.7 degree) and TM (74.1 degree) stages.

126

127 **4. Discussion**

128 Study findings

129 The study has used Numerical model to calculate the lumbar spine curvaturein standing from a 130 healthy subject with a loaded backpack. To our knowledge this is the first time that lumbar spine curvature has numerically been examined. Firstly, the backpack was loaded at 10, 15 and 131 20% of subject's BW (stage 1). This was resulted in G and H angles reduction by about 3.3 132 degree. Chow et al.(2007) found these changes about 3.75 degree. Our numerical model led to a 133 134 good G angle correlation with the previous similar literature values (r = 0.88), in addition a good correlation (r = 0.91) was achieved for H angle. These good correlation factors between our 135 numerical method and previous experimental study can validate our simulation technique. 136 Secondly, three boxes (4, 4 and 12 Kg in weight) were attached in the backpack (stage 2). They 137 were arranged in the sagittal, frontal and transversal planes and the position of the heavier 138 139 weight was changed at each phase. The G angle peaks were observed at stages of SM (23.9 degree), FL (25.1 degree), FR (25.1 degree) and TF (24.6 degree). Similarly, The H angle peaks 140 141 were observed at stages of SM (74.4 degree), FL (76.0 degree), FR (76.0 degree) and TF (75.4 142 degree). Also, the most reduction in lumbar angle is observed at incorrect backpack carrying methods atSBcase that this means flattening in lumbar lordosis. Despite the use of a simplified 143

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model, our predicted values of G and H angles changes were approximately to within 88% of 144 145 the values of experimental-measured reported in the literature (Chow et al, 2007). The numerical model reliably predicted lumbar spine curvature over a range of different loads. 146 Predictions of around 88% of experimental measurement(Chow et al, 2007) would present 147 148 limitations in clinical use, therefore, linear correlations have been used. This enables estimations derived from our simulation to be obtained which are highly accurate (e.g. r = 0.88 149 150 and 0.91 for G and H angles, respectively). 151 This study demonstrates the feasibility of obtaining a range of variable boundary conditions 152 (e.g. altered due to changing the location of the heavier box) and applying a simplified three-153 dimensional model that can predict lumbar spine curvature changes in relatively short solution 154 time. **Comparison to literature and validation** 155 156 Following a literature search we have not found a previous comparable numerical study that 157 used numerical approach to predict lumbar spine curvatureat different conditions of loading. In 158 our study, subject specific G and H angles , measured between three adjacent markers as the 159 curvature for that load, were predicted at a range of loading. However, our study compares 160 well to the experimental study used to predict lumbar spine curvature for a subject in standing 161 with a loaded backpack. Regression analysis between our numerical predictions and similar previous literature (Chow et 162

and 5b). Therefore, there was a strong correlation between the two methods and similar values

al, 2007)led to a correlation gradient of 0.88 and 0.91 for G and H angles, respectively (Figs5a

were predicted. These regression analysis enable true values to be calculated from predicted
model data (using the equations provided in figs5a and 5b). As can be seen in figure 3, there is a
linear relationship between changes of our predicted G and H values and the changes of
percentage of BW. This is in good agreement with the Chow et al (2007) findings. However, the
mean differences of 3.4 and 8.1 degree are observed for G and H angles values respectively.

170 As shown in figure 4, The relationship between G angle and H angle of our numerical simulation has a good correlation which was calculated using a quadratic polynomial equation. This also is 171 in good agreement with Chow et al findings (Chow et al, 2007) (Fig 4). As noted by Motmans et 172 al. (2006), with a load on the back, the combined center of gravity of the trunk plus the 173 174 backpack shifts backward. This creates an extension moment (Bobet and Norman, 1984). In order to counterbalance the weight on the back, a Trunk forward lean occurs (Al-Khabbaz et al, 175 176 2008; Filaire et al, 2001; Goh et al, 1998; Heather et al, 2009; Motmans et al, 2006; Pascoe et al, 177 1997; Singh et al, 2009). A forward displacement can already be seen with loads less than 10% BW (Grimmer et al, 2002). All these are in agreement with our results in the region of lumbar 178 179 spine.Grimmer et al. (2002) reported that when backpack was positioned at T7 level produced 180 the largest trunk forward lean that is in good agreement with our results when heavy box was 181 located in SM. However, low load placement resulted in greater postural adaptations than high 182 load placement (Heather et al, 2009). Nevertheless, Stuempfle et al. (2004) proposed high load 183 placement (ST) considering physiological factors and muscle activities that is in contrast to our findingsat stage 2. Lots of articles have found thatbackpack's COG should be as close as possible 184 to trunkdue to he least load momentum, energy consumption and spine displacement as well 185

186 as m	aintain balance	(Devroey	/ et al, 20	07; Legg&Mahar	ity, 1985; Mo	tmans et al,2006;
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187 Stuempfle et al, 2004). This is in agreement with our results in Transversal plane.

188 Limitations and future trends

We only have reported the lumbar spine curvature. This is mainly because that review of the
surveys shows the importance of LBP on adolescents and its relation to the load carrying (SheirNeiss et al, 2003). Hence this study focused on lumbar region to be paid more attention to it.
Motmans et al. (2006) concluded that, reduced erector spinae EMG activity and increased
Rectus abdominis muscle activity in backpack carrying are disproportionate and asymmetric
with increasing backpack load and Finneran et al. (2003) remarked that such condition is similar
to acute or chronic LBP patients.

Korovessis et al. (2004) researched the relevance of backpack carriage with anthropometric 196 parameters (gender, height, weight) scoliosis, kyphosis in thoracic, lordosis in lumbar and 197 198 sports activities; also its effect on LBP and Dorsal Pain (DP) in children and adolescents between 9-15 years old. After investigating the influence of various factors on LBP he stated that there 199 200 are many potential impacts on spine symptoms so discovering the direct causal relevance 201 between load carrying and LBP is difficult.But Goh et al. (1998) perceived Disproportionate increment in lumbosacral joint force during walking with a backpack. Considering different 202 203 factors, Korovessis et al. (2004) are not very farfetched but the effect of carrying backpack on 204 LBP cannot be ignored specially in adolescents whose spine is growing and getting stronger (Heather et al, 2009; Sheir-Neiss et al, 2003). 205

A 15 years old boy was selected for modeling on account of growing spine at this age which is 206 207 formable with personal habits and they are nonetheless an 'at-risk' group as well (Chow et al, 2007). Also, Korovessis et al. (2004) obtained the most LBP prevalence for 15 years old boys. 208 But it should be noticed that children findings cannot be generalized to adults (Grimmer et al, 209 210 2002). Furthermore, Hong Y and Li (2005) surveyed the role of age difference in trunk kinematics at different loads of 6-12 years old children, perceived larger TFL amplitude in 12 211 years old children. Gender influence should be notified in the future as well; according to 212 213 results of Korovessis et al. (2004), girls experienced more LBP and DP than boys. Reviewing the 214 scientific research reveals the importance of changes in any part of spine in carrying backpack 215 which should be notified in subsequent studies. This study was carried out in static condition and the impact of time and consequent fatigue was ignored. 216

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5. Conclusion:

We have introduced a simulated model of lumbar spine which was able to reliably predict the 219 lumbar spine curvature in standing from a healthy subject with a loaded backpack. Strong 220 221 correlation were determined for our prediction and similar experimentally literature (R = 0.88for G angle and R=0.91 for H angle) which enables correction of the numerical values predicted 222 223 using regression equations. The model developed was used to make predictions while the 224 backpack was loaded with three boxes (4, 4 and 12 Kg in weight) arranged in the sagittal, frontal and transversal planes and the position of the heavier weight was changed at each 225 phase. The G and H angle peaks were similarly observed at stages of SM, FL, FR and TF. The most 226

- reduction in lumbar angle is also observed at incorrect backpack carrying postures in SB.The
- advantage of using a simple model was the relatively quick solution time.

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230 References
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- 231 Chow, D. H. K., Leung, K. T. Y. and Holmes, A. D. (2007): Changes in spinal curvature and
- 232 Proprioception of schoolboys carrying different weights of backpack. Ergonomics. 50(12), 2148
- 233 2156.
- 234 Motmans, R. R. E. E., Tomlow, S. and Vissers, D. (2006):Trunk muscle activity in different modes
- of carrying schoolbags. Ergonomics. 49(2), 127 138.
- Reid, SA, Stevenson, JM and Whiteside, RA (2004): Biomechanical assessment of lateral
- stiffness elements in the suspension system of a backpack. Ergonomics. 47(12), 1272 1281.
- 238 Singh, T. and Koh, M. Koh. (2009): Effects of backpack load position on spatiotemporal
- parameters and trunk forward lean. Gait & Posture. 29, 49–53.
- 240 Stephanie A. Southard, Gary A. Mirka.(2007): An evaluation of backpack harness systems
- in non-neutral torso postures. Applied Ergonomics. 38, 541–547.
- 242 Bahraseman HG, Hassani K, Navidbakhsh M, Espino DM, Sani ZA, Fatouraee N. (2013): Effect of
- exercise on blood flow through the aortic valve: a combined clinical and numerical study.
- Comput Methods Biomech Biomed Engin, In Press. DOI: 10.1080/10255842.2013.771179.

- Al-Khabbaz, YSSM, Shimada, T. and Hasegawa, M. (2008): The effect of backpack heaviness on
- trunk-lower extremity muscle activities and trunk posture. Gait & Posture. 28, 297- 302.
- 247 Skaggs DL, Early SD, D'Ambra P, Tolo VT, Kay RM. (2006): Back pain and backpacks in school
- children. J PediatrOrthop. 26(3), 358-63.
- Mackie HW, Legg SJ, Beadle J, Hedderley D. Comparison of four different backpacks intended
 for school use. ApplErgon. 2003 May;34(3):257-64.
- 251 Rashed LA, Hawas HA, Hozaim NA. (2005): Effect of Different Types of Bag on Balance & Center
- 252 of Gravity, [dissertation], KING SAUD UNIVERSITY.
- 253 Devroey C, Jonkers I, de Becker A, Lenaerts G, Spaepen A. (2007): Evaluation of the effect of
- backpack load and position during standing and walking using biomechanical, physiological and
- subjective measures. Ergonomics.50(5), 728-42.
- Abe D, Muraki S, Yasukouchi A. (2008): Ergonomic effects of load carriage on the upper and
- lower back on metabolic energy cost of walking. ApplErgon. 39(3), 392-8.
- 258 Stuempfle KJ, Drury DG, Wilson AL. (2004) Effect of load position on physiological and
- 259 perceptual responses during load carriage with an internal frame backpack. Ergonomics. 47(7),
- 260 784-9.
- 261 Reid, SA, Stevenson, JM and Whiteside, RA (2004): Biomechanical assessment of lateral
- stiffness elements in the suspension system of a backpack. Ergonomics. 47(12), 1272 1281.

263	Hamish W. Mackie, Joan M. Stevenson, Susan A. Reid, Stephen J. Legg. (2005): The effect of
264	simulated school load carriage configurations onShoulder strap tension forces and shoulder
265	interface pressure. Applied Ergonomics. 36, 199–206
266	
267	Grimmer K, Dansie B, Milanese S, Pirunsan U, Trott P. (2002): Adolescent standing postural
268	response to backpack loads: a randomised controlled experimental study. BMC
269	MusculoskeletDisord. 17, 3:10.
270	
271	Lloyd R, Parr B, Davies S, Cooke C. (2010): Subjective perceptions of load carriage on the head
272	and back in Xhosa women. Applied Ergonomics. 41, 522–529.
273	
274	Leilnahari K, Fatouraee N, Khodalotfi M. (2011): Spine alignment in men during lateral sleep
275	position: experimental study and modeling, Biomed Eng Online.10, 103.
276	
277	Bobet J, Norman RW.(1984): Effects of load placement on back muscle activity in load carriage.
278	European Journal of Applied Physiology. 53, 71 – 75.
270	Descen DD, Descen DE, Mang VT, Shim DM, Kim CK (1007), Influence of corruing book base on
279	Pascoe DD, Pascoe DE, wang YT, Shim DW, Kim CK.(1997): Influence of carrying book bags on
280	gait cycle and posture of youths. Ergonomics, 40: 631–641.
281	Filaire M, Vacheron JJ, Vanneuville G, Poumarat G, Garcier JM, Harouna Y, Guillot M, Terver S,
282	Toumi H, Thierry C.(2001): Influence of the mode of load carriage on the static posture of the

pelvic girdle and the thoracic and lumbar spine in vivo. Surgical and Radiologic Anatomy. 23,
27–31.

285 Goh J-H, Thambyah A, Bose K. (1998): Effects of varying backpack loads on peak forces in the

lumbosacral spine during walking. Clinical Biomechanics. 13(1), S26–31.

287 Heather M. Brackley, Joan M., Stevensonand Jessica C. Selinger. (2009): Effect of backpack load

placement on posture and spinal curvature in prepubescent children. Work. 32, 351–360

289 Grimmer, K., DANSIE, B., MILANESE, S., PIRUNSAN, U. and TROTT, P. (2002) Adolescent standing

290 postural response to backpack loads: a randomised controlled experimental study. BMC

291 MusculoskeletDisord. 3, 10.

Haex B. (2004): Back and bed. Ergonomic aspect of sleeping. 2 editions. New York: CRC press.

Legg, S.J., Mahanty, A.(1985): Comparison of five modes of carrying a load close to

the trunk. Ergonomics. 28 (12), 1653–1660.

295

296 Sheir-Neiss GI, Kruse RW, Rahman T, Jacobson LP, Pelli JA. (2003) The association of backpack

use and back pain in adolescents. Spine. 28(9), 922-30.

298

- 299 FINNERAN, M.T., MAZANEC, D., MARSOLAIS, M.E., MARSOLAIS, E.B. and PEASE, W.S. (2003):
- Large-array surface electromyography in low back pain: a pilot study. Spine, 28, 1447–1454.

- 302 Korovessis P, Koureas G, Papazisis Z. (2004): Correlation between Backpack Weight and Way of
- 303 Carrying, Sagittal and Frontal Spinal Curvatures, Athletic Activity, and Dorsal and Low Back Pain
- in Schoolchildren and Adolescents. J Spinal Disord Tech.17(1), 33-40.
- 305
- Hong Y, Li JX. (2005): Influence of load and carrying methods on gait phase and ground
- reactions in children's stair walking. Gait and Posture. 22(1),63–8.
- 308
- 309 **Tables:**

310	Table 1 Abbreviations	for the nositio	n of heavier hoy i	(12 Ko) at	different nlans
210		ior the position		(בב <i>הצ</i>) מו	Lunierent plans.

Plane	Sagittal			Frontal			Transverse		
		In the	In		In the		The	In the	The
	In top	middle	bottom	In left	middle	In right	nearest	middle	farthest
	of two	of two	of two	of two	of two	of two	box to	of two	box to
	other	other	other	other	other	other	the	other	the
Heavier BoxPosition	boxes	boxes	boxes	boxes	boxes	boxes	body	boxes	body
Abbreviation	ST	SM	SB	FL	FM	FR	TN	TM	TF

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	0% of BW		10% c	10% of BW		15% of BW		20% of BW	
	Chow et		Chow et		Chow et		Chow et		
	al.(2007)	Present	al. (2007)	Present	al. (2007)	Present	al. (2007)	Present	
Angle	findings	study	findings	study	findings	study	findings	study	
G									
(T12-L3-S1)	21.6	28.1	18.9	27.3	18.2	25.9	17.8	24.8	
Н									
(L3-S1-horizon)	76.9	79.1	75.1	78.9	74.3	77.1	73.2	75.8	

Table 2. The lumbar spine angles at different backpack loads. Note, BW refers to Body weight.

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317

318 **Table 3.** The lumbar angles at different location of heavier load (12 Kg) in sagittal, frontal and

319 transverse planes.

Location of									
heavier load	ST	SM	SB	FL	FM	FR	TN	TM	TF
G angle									
(T12-L3-S1)	23.2	23.9	22.9	25.1	24.4	25.1	24.1	24.4	24.6
H angle									
(L3-S1-horizon)									
	73.4	74.4	72.9	76.0	75.1	76.0	74.1	74.7	75.4

320	Figure	captions:
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- 321 **Figure 1.** The model of subject with a backpack.
- **Figure2.** The model with weights located on sagittal, frontal and transverse plans.
- **Figure 3.** G (L3-S1-horizon) and H (T12-L3-S1) angles changes due to variation in amount of
- 324 backpack load.
- **Figure 4.** The relationship between G (L3-S1-horizon) and H (T12-L3-S1) angles.
- 326 **Figure 5.** Regression analysis between numerical predictions of and similar previous literature
- for G (L3-S1-horizon) (Fig 5a) and H (T12-L3-S1) (Fig 5b) angles.

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329

330 Fig 1



333 Fig 2



335 Fig 3









